



Resolving Gender Difference in Problem Solving Based On the Analysis of Electroencephalogram (EEG) Signals

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Abstract: Problem solving is regarded as one of the core work-related abilities and skills, which are highly demanded by the workplace and industry. Current literature suggests that problem solving abilities might differ from one individual to another due to biological factors such as brain activation, cognitive functions and hormones, as well as due to socio-cultural and socio-economic factors like gender roles, self-perceptions and stereotyping. Hence, this study used electroencephalogram (EEG) signals to investigate the differences in problem solving skills among the Malaysian undergraduates based on their gender differences. 29 undergraduate students from the Faculty of Electrical Engineering, Universiti Teknologi Malaysia (UTM) served as the subjects of the experiments in this research. Specifically, 16 female and 13 male subjects engaged in two main problem-solving tasks: mental arithmetic task and Tower of Hanoi (TOH) task. The EEG data were analysed using partial directed coherence (PDC) and power spectrum estimation (PSE). Based on the results, female subjects achieved only 1% higher performance in mental arithmetic task, while male subjects achieved about 13% higher performance in TOH task. The differences in terms of the functional connectivity between brain regions, i.e. in PDC, as well as the power distribution of 6 EEG waveforms, i.e. delta, theta, alpha, beta, gamma and high gamma bands are also highlighted and represented graphically in this paper.

Keywords: Problem solving, electroencephalogram (EEG) signals, gender differences, partial directed coherence (PDC), power spectrum estimation (PSE).

1. Introduction

Within the area of human cognition, problem solving is considered to be "higher-layer cognitive process" (Wang & Chiew, 2010, p.81). As explained by the authors:

Problem solving is a cognitive process of the brain that searches a solution for a given problem or finds a path to reach a given goal. When a problem object is identified, problem solving can be perceived as a search process in the memory space for finding a relationship between a set of solution goals and a set of alternative paths. (ibid.)

In order to meet the demands and expectations of the real workplace, graduates need to equipped themselves with “work-related practical skills or competences that current employees (or prospective new hires) are able to use in order to perform various job tasks successfully” (World Economic Forum, 2016, p.18). Among the core work-related abilities and skills needed to accommodate the fourth industrial revolution is problem solving, which also one of the elements of higher order is thinking skills heavily emphasized by academic curriculum across the world.

In examining undergraduates' problem solving task by the use of brain functional connectivity, a number of fundamental concepts were suggested by the neuropsychological literature. The first concept acknowledges the fact that the initial stage of human problem solving is the understanding of the problem. Within this stage of problem identification, the elements of attention, mental representation of the problem and situated cognition need to be considered. This is in line with the conceptualisation of problem solving as a complex mental process resulted from “the culmination of all the process that make up (individuals) cognitive arsenal (which include) perception, pattern recognition, attention and immediate memory, language, and decision making” (Robinson-Riegler & Robinson-Riegler, 2012, p.494). Another crucial concept in problem solving is the strategies utilised, which include the analogy approach, the means-end heuristic and the hill-climbing heuristic (Matlin, 2014).

Past literature has suggested the differences between males and females in terms of cognition functions (Bell et al., 2006; Miller & Halpern, 2014; Weiss et al., 2003). Males and females might demonstrate the same cognitive performance but mentally they were actually gone through different information processing paths (Gong, He & Evans, 2011; Iddon & Williams, 2009; Jewel, 2009). Moreover, through numerous experiments, it was found out that females could perform better in some tasks compared to males. For instance, females tend to be better than males in linguistic tasks, are better in autobiographical memory and are more multitasking than males (Iddon & Williams, 2009; Weiss et al., 2003; Thilers, MacDonald & Herlitz, 2007). Males on the other hand outperformed women in visuo-spatial tasks like mental rotation and mathematical reasoning (Iddon & Williams, 2009; Weiss et al., 2003; Thilers, MacDonald & Herlitz, 2007). Furthermore, the differences of males and females could also be accessed through their creativity (Razumnikova, 2004).

With reference to brain differences, a longitudinal study by Raznahan et al. (2010), for instance, revealed that sex hormones influence some specific aspects of brain development during puberty. The study provided the evidence that “adolescence (n=284) with higher androgen sensitivity showed more male-typical patterns of maturation in specific areas of the cerebral cortex” (Miller & Halpern, 2014, p.40. Such finding led to insights into cognitive sex differences mainly because the cerebral cortex supports most cognitive functioning. On the other hand, the authors also highlighted findings from other studies by Jausovec and Jausovec (2012) and Lenroot and Giedd (2010) which indicated that “women and men sometimes use brain regions differently to achieve equal cognitive performance” [ibid.].

It is suggested that gender differences in cognition functions is also due to the socio-cultural aspect of gender roles that resulted in other gender specific elements such as self-perceptions and stereotyping (Miller & Halpern, 2014; Weiss et al., 2003). From the aspect of cultural differences, studies on gender or sex differences in mathematics tests (e.g. Else-Quest, Hyde, & Linn; 2010; Kane & Mertz; 2012) challenged the universal idea of male advantages in mathematics as sex difference varied across socioeconomic levels of families and countries. For instance, it is found that males who belonged to families with higher socioeconomic status (e.g. Levine et al., 2005; Penner & Paret, 2008) and those who are living in wealthier countries (e.g. Lippa, Collaer, & Peters, 2010; Reilly, 2012) have more advantages in spatial (and mathematics) performance.

Engagement in sex-typed activities further explained the development of spatial skills among males. For example, spatial skills can be improved by playing construction toys or action video games that are male-typical activities (e.g. Miller & Halpern, 2014; Uttal et al., 2013). Research like one by Haier et al. (2009) further added that such male-typical activities could also caused neural changes in cortical thickness, as well as ex-differentiated patterns of brain activation.

Despite extensive studies on brain connectivity conducted by a number of Malaysian researchers (Hashim et al., 2015; Kosnan, Safri & Khalid, 2015; Safri et al., 2008), it was found that less work had been done in incorporating neuropsychological concepts into that particular research area. Based on these observations, the researchers strongly believe that to explore brain functional connectivity from the neuropsychological perspective within the local subjects was worth researching on. In fact, Matlin (2014) suggested that problem solving strategies are contextualised and that researchers should consider individual and cultural differences when attempting to explore this dimension.

Owing to the gap within the Malaysian literature and having been guided by the recent and relevant literature within the neurocognitive aspect of problem-solving, this research seeks to identify the differences of performance based on brain functional connectivity with regards to gender of the Malaysian subjects. Hence, guided by the science of cognitive sex differences as emphasised by Miller and Halpern (2014), this research aimed to examine the Malaysian undergraduates' problem solving ability from the neurocognitive approach that specifically focuses on brain functional connectivity.

The analysis for structure of the brain begins with the identification of the various functional parts of the brain with their interconnections (Park & Friston, 2013). Each functional part is referred as a node where the interconnection

between each node can be defined by three types of connectivity: structural connectivity, for anatomical links; functional connectivity, for undirected statistical dependencies; and effective connectivity, for directed causal relationships among distributed responses Friston (1994). Functional connectivity is generally inferred by the correlation between nodal activities on the basis of blood oxygenation level-dependent (BOLD) functional MRI (fMRI) or coherence in electro- or magnetoencephalogram (EEG/MEG) signals.

EEG is one of techniques used to measure the electrical activity of the brain at different sites of the head. This is typically using electrodes placed on the scalp, i.e. by using cap electrode. One of its main benefits over other brain signal recording techniques are its high temporal resolution and the fact that it can be recorded noninvasively (Freeman & Quiroga, 2013). EEG is a very accessible and useful tool for the analysis of high level brain processes since it is relatively low cost and widely used both in clinical settings and research laboratories (ibid.)

Past literature suggested that EEG has been used on healthy participants or subjects in studies related to brain mapping (e.g. Tóth et al., 2017; Wens et al., 2015), within studies that examined the nature of brain connectivity in terms of its structure and functions (e.g. Allen et al., 2018; Amico et al., 2017; Chu et al., 2015; Hardmeier et al, 2014), as well as studies related to specific clinical conditions involving sleep patterns (e.g. Miraglia et al., 2018), or during a particular intervention (e.g. Myers et al., 2015). Within the clinical setting, EEG has also been utilised to study brain functional connectivity in research involving patients with certain diseases (e.g. Nunez, Srinivasan & Fields, 2015), autism (e.g. Righi et al., 2014), epilepsy (e.g. Adebimpe et al., 2016; Lagarde et al., 2018; Sargolzaei et al., 2015), dyslexia (e.g. González et al., 2018), Alzheimer’s disease (e.g. Engels et al., 2015; Vecchio et al., 2017; Yu et al., 2016), Parkinson’s disease (e.g. Yuvaraj et al., 2016), and schizophrenia (e.g. Damaraju et al., 2014).

2. Methodology

2.1 Subjects

In this study, 29 healthy undergraduates from the then Faculty of Electrical Engineering (now School of Electrical Engineering), Universiti Teknologi Malaysia (UTM) served as the subjects. They consisted of 16 female and 13 male students. This as to accommodate the suggestions by Matlin (2014) that problem solving strategies are contextualised and that researchers should consider socio-cultural differences when attempting to explore this dimension. In this study, the subjects’ educational background was the main socio-cultural variable that was taken into consideration. The number of subjects was also aligned with other past studies conducted within the Malaysian context (e.g. Hashim et al., 2015; Kosnan, Safri & Khalid, 2015). The selection of subjects was based on convenience sampling approach. Those who volunteered to participate in the experiment were given choices to choose preferred time slots based on the schedules that the researchers provided.

2.2 Research Design

In order to gather the data, experimental research was used. Specifically, repeated measure design was employed to allow the same subjects to experience the same control and experimental conditions (Shaughnessy & Zechmeister, 1997). Through such method, subjects’ cognitive abilities can be explored and compared (Elmes, Kantowitz & Roediger, 2012).

2.3 Measurement

The experiment began with the researchers gaining approvals from the subjects through informed consent. Subjects were given a brief explanation regarding the terms and conditions in proceeding experiment as well as the experimental procedure (Priscilla, 2014). They were then set up with EEG instrument. The experiment was conducted inside a laboratory room where the room was equipped with natural experiment setting with limited users, in order to avoid any extraneous environment disturbance. The subject’s head was attached with EEG electrode and the signals were recorded using NeuroFax EEG 9000 signal acquisition software. The electrode placement for each subject is shown in Figure 1 while the experiment procedure flow chart is shown in Figure 2.

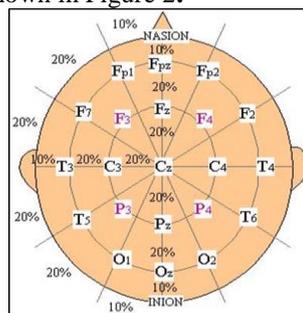


Fig. 1: Electrode label points based on the 10/30 electrode placement system

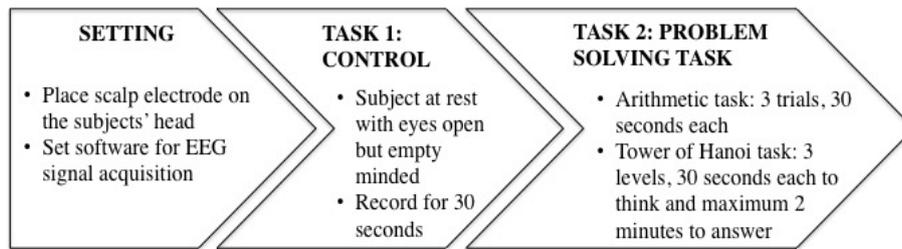


Fig. 2: The experimental procedure

The labeling electrodes placements were based on adjacent brain areas which the letter represented structural brain regions identification (Priscilla, 2014). The number besides the letter signified the position of the placements on the head where odd numbers represented left side of the head and even numbers represented right side of the head (Trans Cranial Technologies, 2012). Table 1 illustrates the electrodes labeling letters that represent the brain regions.

Table 1: Electrodes labeling representing brain regions

Electrode	Brain Region
F	Frontal
T	Temporal
C	Central
P	Parietal
O	Occipital

For the control task, subjects were required to be at rest and relax, and if possible with emptied mind. The subjects were asked to open their eyes during this task to meet the requirement of the recordings. The control task was recorded for 30 seconds for one to three times depending on a subject's mental condition (for instance, nervousness) before they proceeded with the problem solving task.

The problem solving task consisted of two sub tasks: the arithmetic task and the Tower of Hanoi (TOH) task. In the arithmetic task, subjects were asked to mentally subtract 7 from 1000 continuously within 30 seconds. The final answer for each trial was noted and the process was repeated for three trials after resting for about 30 seconds per trial. EEG signals were recorded while the subjects were engaging in the thinking process.

Finally, the TOH task was divided into three difficulty levels: easy, medium and hard. The levels were chosen based on the feedback from subjects of the preliminary experiment. EEG signals were recorded when subjects were engaging in thinking (i.e. 30 seconds) and while solving the puzzle (i.e. maximum of two minutes). The rest time interval for each level was also 30 seconds. Overall, 10 EEG data (.csv) were recorded for each subject and the recorded EEG data were named using short form of the tasks name as shown in Figure 3.

#c	= control task
#a1	= arithmetic task trial 1
#a2	= arithmetic task trial 2
#a3	= arithmetic task trial 3
#et	= TOH task easy level (think)
#ea	= TOH task easy level (answer)
#mt	= TOH task medium level (think)
#ma	= TOH task medium level (answer)
#ht	= TOH task hard level (think)
#ha	= TOH task hard level (answer)

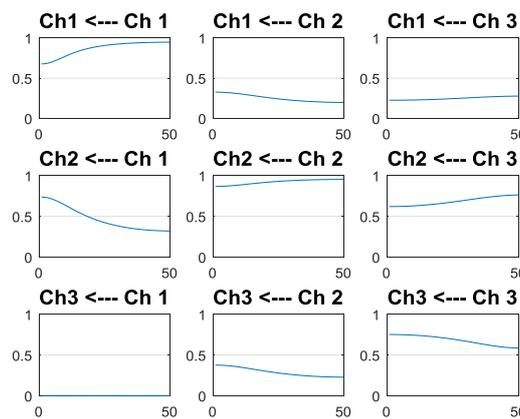
Fig. 3: Codes for recorded EEG data

The EEG signal is first analysed to determine the functional connectivity between the various areas of the brain using partial directed coherence (PDC) method followed by the distribution of power in frequency using power spectrum estimation (PSE). The concept of PDC proposed in Teplan (2002) is a frequency domain method that represents a multivariate autoregressive (MVAR) process. Conceptually, PDC analysis is performed to illustrated interactions between time direction and spectral properties signal at the brain (Teplan, 2002). Granger causality principle can be expressed in terms of the MVAR that states if some time series $y[n]$ contains information in past terms that helps in the prediction of series $x[n]$, then $y[n]$ is said to cause $x[n]$. An illustration of how PDC analysis is performed on a 3 equations MVAR process is shown below. Suppose a MVAR process is defined by the following sets of equations:

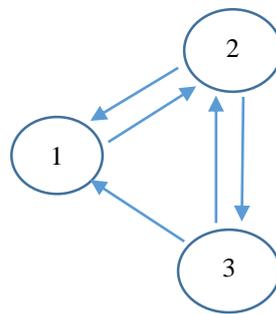
$$\begin{aligned}
 x_1[n] &= 0.5x_1[n-1] + 0.3x_2[n-1] + 0.4x_3[n-1] + v_1[n] \\
 x_2[n] &= -0.5x_1[n-1] + 0.3x_2[n-1] + x_3[n-1] + v_2[n] \\
 x_3[n] &= -0.3x_2[n-1] - 0.2x_3[n-1] + v_3[n]
 \end{aligned} \tag{1}$$

where $x_1[n]$, $x_2[n]$ and $x_3[n]$ represent the MVAR process at node 1, 2, and 3 which are driven by additive white Gaussian noise sources $v_1[n]$, $v_2[n]$ and $v_3[n]$. These equations represent the MVAR process show the correlation between each node 1, 2 and 3 except that for $x_3[n]$ there is no correlation with $x_1[n]$. In general, $x[n]$ with conjunction at $y[n]$ in MVAR determines the directional functionality. Thus, $x[n]$ is operated as information sources that bidirectional functional connectivity to $y[n]$ is regarded as information sink.

Using the MVAR model defined in Equation (1), PDC analysis is performed using the method defined in (Takahashi, 2007) and the results shown as a 3 x 3 matrix layout as shown in Figure 4a). The diagonal terms are not considered in the PDC analysis since it represents an interaction between a signal with itself. Thus, it is of interest to look for interactions for two different signals based on an acceptable magnitude. For discussions on the interpretation of PDC analysis is described in (Takahashi, 2007). Actual magnitude is obtained from prior knowledge of the characteristics of the signal interaction. From an acceptable magnitude of 0.1 for this example, functional connectivity does not occur only for $x_1[n]$ to $x_3[n]$. The resulting functional connectivity diagram is shown in Figure 4b). Since 19 electrodes are used in the 10/30 electrode placement system, the resulting matrix layout is 19 x 19 with a total of 19 elements in the functional connectivity diagram.



(a) PDC analysis



(b) Functional connectivity

Fig. 4: PDC analysis results shown in a 3 x 3 matrix layout and the derived functional connectivity. [Ch 1 refers to $x_1[n]$, Ch2 refers to $x_2[n]$ and Ch3 refers to $x_3[n]$; vertical axis represents magnitude and horizontal axis represents frequency in samples].

The distribution of EEG signal power is segregated according to the following frequency bands: delta (0-4 Hz), theta (4-8 Hz), alpha (8-13 Hz), beta (13-31 Hz), gamma (31-51) and high gamma (51-120 Hz) (Dai, 2017; Omidvarnia, 2011). How much the power is distributed over the frequency band very depends on the performed task. For example, a high level in the gamma frequency band relates to active thinking. Thus, PSE can be utilized to determine how the power of the EEG signal is distributed over the frequency band. The most basic method for PSE is the periodogram which is defined as follows (Proakis, 2006).

$$S_x[k] = \frac{1}{N} \left| \sum_{n=0}^{N-1} x[n] e^{j \frac{2\pi kn}{N}} \right|^2 \quad (2)$$

where $x[n]$ is the signal of interest in discrete-time representation, and N is the duration of the signal. Since the periodogram is not an efficient estimator, alternative methods are considered which reduces the variance in the PSE as the signal length is increased. The Welch PSE is such a method and is utilized in this study (Proakis, 2006). An N length signal $x[n]$ is segmented into length of M samples where the total number of sub-segments is $L=N/M$. The segmented signal can be expressed as

$$x[n] = [x_0[n] \ x_1[n] \ \dots \ x_l[n] \ \dots \ x_{L-1}[n]] \quad (3)$$

For each segment, the PSE is calculated similar to Eq. 3

$$S_{x,l}[k] = \frac{1}{M} \left| \sum_{n=0}^{M-1} w[n] x_l[n] e^{j \frac{2\pi kn}{M}} \right|^2 \quad (4)$$

where $w[n]$ is the window function. Any window function such as Hamming or Bartlett window can be utilized for this purpose. Once all the PSE for each segment is calculated, the average PSE is obtained by

$$S_{x,welch}[k] = \frac{1}{L} \sum_{l=0}^{L-1} S_{x,l}[k] \quad (5)$$

Overlapping of segments can be applied for the Welch PSE. If 50 percent is used, effectively the total number of segments doubles that results in reducing the variance in PSE by half compared to non-overlapping segments.

3. Results

In this study, analyses of data were conducted based on two outputs from the experiment, i.e. the tabulated answer and the performances of subjects, and the recorded EEG data (.csv) during the tasks. The tabulated answer and performance of subjects refer to the subjects' abilities in answering the given arithmetic questions with accurate final value for each trial. This also included their abilities to complete the TOH task within the maximum of two minutes provided for each level. Based on this, comparison for gender factors can be made by calculating the statistics of high performance versus low performance subjects as shown in Tables 2 and 3. It is further represented in a graphical form as in Figures 5 and 6.

In contrast, the recorded EEG data were analyzed using two methods, namely partial directed coherence (PDC) and power spectrum estimation (PSE) methods. The PDC analysis provided a more visual comparison based on the information pathway between the channels or brain regions of subjects when doing the given tasks. On the other hand, the PSE method analysed the change in power distribution of the EEG waveforms. In this project, both the PDC and PSE outputs were obtained on C-program running on a Linux platform. The outputs were further analysed using Microsoft Excel (for t-test) and Paint (for drawing).

Table 2: Subjects' performance statistics for female subjects

Tasks	4FRH	4FLH	1FRH	1FLH	ΣF	%	Overall	Overall (%)
a1	3	2	2	2	9	56.25	30	62.5
a2	2	2	2	4	10	62.53		
a3	3	4	2	2	11	68.75		
ea	4	4	4	4	16	100	28	58.33333
ma	4	3	2	2	11	68.75		
ha	0	0	0	1	1	6.25		

Table 3: Subjects' performance statistics for male subjects

Tasks	4FRH	4FLH	1FRH	1FLH	ΣF	%	Overall	Overall (%)
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a1	4	1	2	1	8	61.53846		
a2	4	0	2	1	7	53.84615	24	61.53846
a3	3	2	3	1	9	69.23077		
ea	4	2	4	3	13	100		
ma	3	1	4	3	11	84.61538	28	71.79487
ha	2	0	1	1	4	30.76923		

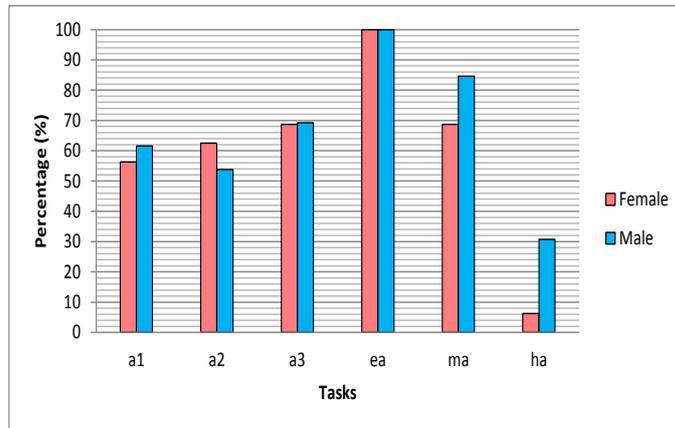


Fig. 5: Graph of gender performances (%) against tasks: all trials

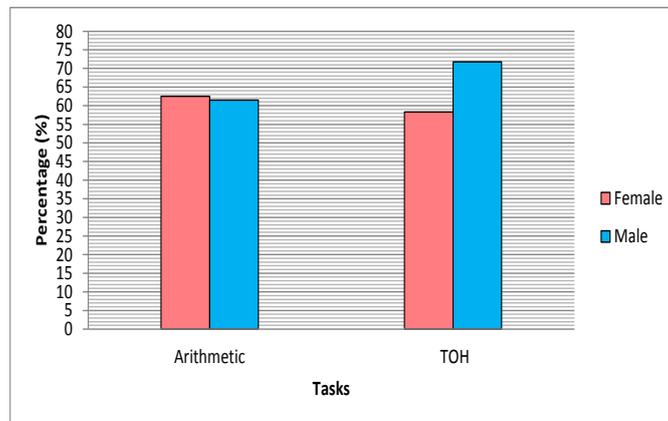


Fig. 6: Graph of gender performances (%) against tasks: overall tasks

4. Discussions

4.1 PDC Analysis

Using the methodology described in Section 2.3, the PDC output was plotted in the form a 19x19 matrix layouts of all the 19 channels used during EEG data recording for the 29 subjects and tasks. Figure 7 shows an example of function connectivity pattern for subject 1 while doing arithmetic task a1 and a2. For all functional connectivity patterns shown in this paper, the source for the signal is labeled as yellow while the sink for the signal is labeled as blue for male subject and pink for female subject respectively. Referring to task a1, the signal source is from the F2 region and the signal source for task a2 is from T4 region. Due to the large number of patterns, it is not possible to discuss each pattern for a given subject and task. The approach taken in this analysis is tabulate the signal sources according to task and gender as shown in Tables 4 and 5, and determine if there is any difference in the distribution of signal sources source from the functional connectivity pattern.

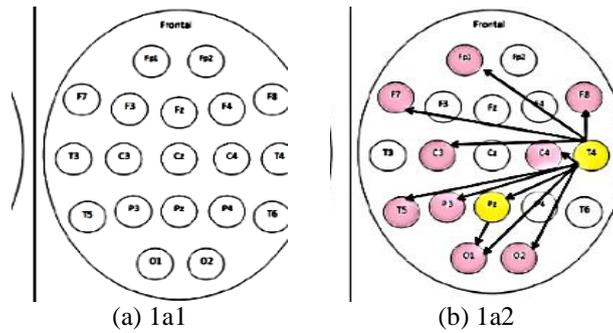


Fig. 7: Functional connectivity diagram for respondent 1 of task a1 and a2

Basically, the functional connectivity pattern for problem solving should originate mainly from the frontal lobe. The tabulated PDC results have also shown that most of the signal sources for both the male and female subjects are from the frontal (F) regions. The results suggested that the female subjects outperformed the male subjects in arithmetic task while male subjects outperformed female subjects in TOH task.

The summarised signal sources as shown in Table 6 especially proved that the female subjects use more frontal regions in arithmetic task, while the male subjects use more frontal regions during TOH task. This shows that the utilization of the frontal regions as the source of EEG information flow during a task is proportional to the subject’s performance shown in Tables 2 and 3.

Table 4: Gender differences in PDC sources of information pathway for high task performance - Female subjects

a1	a2	a3	et	ea	mt	ma	ht	ha
Fp1, Fp2, F8	F7, F8	Fp2, F3, F7, F8, Fz	Fp1, Fp2, F7, F8	Fp1, Fp2, F7, F8	Fp1, F7, F8	Fp1, F7, F8	F7	F7
T3, T4, T5, T6	T3, T4, T5	T3, T4, T5	T3, T4, T5	T3, T4, T5	T3, T4, T5	T3, T4, T5, T6		T3
	O1	O2	O1, O2	O2	O2	O1		
		Pz	Pz	Pz	Cz			

Table 5: Gender differences in PDC sources of information pathway for high task performance - Male subjects

a1	a2	a3	et	ea	mt	ma	ht	ha
Fp1, Fp2, F7, Fz	Fp1, Fp2, F7	Fp1, F4, F7, Fz	Fp1, Fp2, F7, F8	Fp1, F7	F4, F8	Fp1, F7	F8	
T3	T3, T5, T6	T3, T4	T3, T4	T3, T4, T6	T3, T4, T6	T3, T4, T6	T3, T4	T3, T4
O2	O1	O2	O2	O2				
	Pz				Pz		Pz	Pz

Table 6: Gender differences in PDC sources of information pathway for high task performance - Overall task

Arithmetic Task		TOH Task	
Female	Male	Female	Male
Fp1, Fp2, F3, F7, F8, Fz	Fp1, Fp2, F4, F7, Fz	Fp1, Fp2, F7, F8	Fp1, Fp2, F4, F7, F8
T3, T4, T5, T6	T3, T4, T5, T6	T3, T4, T5, T6	T3, T4, T6
O1, O2	O1, O2	O1, O2	O2
Pz	Pz	Cz, Pz	Pz

4.2 PSE

An example of the power spectrum measured at Fp1 is shown in Figure 8 where the distribution of signal power is segregated as follows bands: delta (0-4 Hz), theta (4-8 Hz), alpha (8-13 Hz), beta (13-31 Hz), gamma (31-51) and high gamma (51-120 Hz). In this example, it is observed that there is significant power at frequency less than 31 Hz indicating brain activities in the delta, theta, gamma and beta bands.

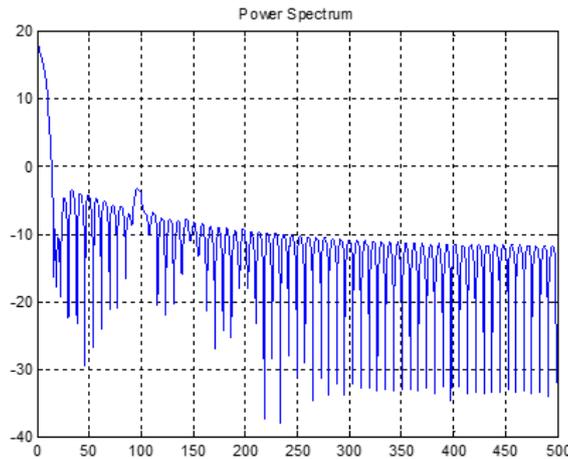


Fig. 8: Example of a power spectrum at Fp1 for a subject while performing a task

The power spectrum for all the subjects, bands and electrodes are compared between the male and female subjects for all the tasks. The example for Fp1 and Fp2 is shown in Figure 9 for the delta band. The horizontal axis represents the tasks defined in Figure 9 while the blue and red bars represent the power measured for the male and female subjects respectively. T-test was used to determine if there was a significant difference between the male and female subjects for all task, electrodes and bands.

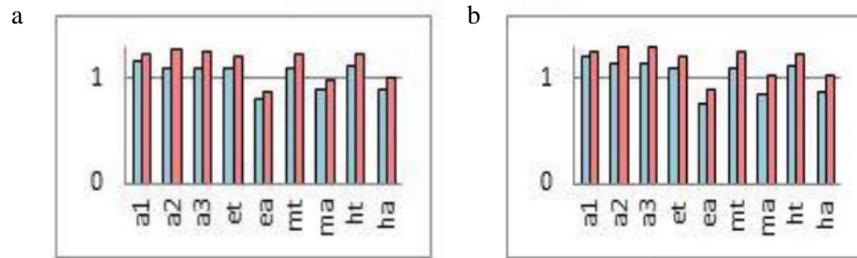


Fig. 9: Comparison between the power in the delta band for Fp1 and Fp2 at state of rest with the various tasks

The gender differences results based on PSE show changes in control task to problem solving tasks ratio for each of the EEG waveform mentioned. For both male and female subjects, the labeled significant difference can be observed mostly at the frontal regions. During arithmetic task, the power of delta and theta band (especially in frontal region) increases for both genders with the decrease in power for the alpha, beta, gamma and high gamma bands. The major frequency band used by the female subjects is the theta band while the male subjects used theta and beta bands especially during the mental arithmetic task. In contrast, during TOH task, there is an increase in power for high gamma band for female subjects, while the power increases in both the gamma and high gamma power bands for male subjects. The difference power over the various bands during the problem solving tasks is directly related to the subjects' performance. For instance, male subjects who showed the best performances in TOH task have correspondingly higher gamma and high gamma power compared to the female subjects.

5. Conclusion

From this study, it can be inferred that the term 'differences in problem solving' not only refers to the ability of an individual to solve a given problem, but also refers to his/her way of thinking, thinking pattern or strategy in a given time to solve an encountered problem in order to reach the desired goal. This is especially when dealing with a close-ended solution problem. Often individuals would reach the same solution for the problem regardless of their gender or background. However, the way each individual solves a certain problem or the time taken for his/her to solve the same problem may differ from one to another.

Hence, the study of gender differences in problem solving highlighted by this study has been conducted by comparing the performance of subjects based on the gender groups (i.e. male and female). The EEG data analysed which involved PDC and PSE were useful to determine the relation between the subjects' performances and the different parts of brain regions involved (as shown in PDC results) and wave power distributions (as shown in PSE results).

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